# Cariostatic effect of fluoride-containing restorative materials associated with fluoride gels on root dentin

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# **ABSTRACT**

econdary caries is still the main cause of restoration replacement, especially on the root surface Objective: This in vitro study evaluated the cariostatic effects of fluoride-containing restorative materials associated with fluoride gels, on root dentin. Materials and Methods: A randomized complete block design was used to test the effects of the restorative systems, fluoride regimes and the interactions among them at different distances from restoration margins. Standardized cavities were prepared on 240 bovine root specimens and randomly assigned to 15 groups of treatments (n=16). Cavities were filled with the following restorative materials: Ketac-Fil (3M-ESPE); Vitremer (3M-ESPE); Dyract/Prime & Bond NT (Dentsply); Charisma/Gluma One Bond (Heraeus Kulzer) and the control, Z250/Single Bond (3M-ESPE). The specimens were subjected to a pH-cycling model designed to simulate highcaries activity. During the cycles, 1.23% acidulated phosphate fluoride, 2.0% neutral sodium fluoride or deionized/distilled water (control) was applied to the specimens for 4 min. The surface Knoop microhardness test was performed before (KHN,) and after (KHN,) the pH cycles at 100, 200 and 300 μm from the margins. Dentin microhardness loss was represented by the difference in initial and final values (KHN, - KHN,). Data were analyzed by Friedman's and Wilcoxon's tests, ANOVA and Tukey's test ( $\alpha$ =5%). Results: The interaction of restorative systems and topical treatments was not significant (p=0.102). Dentin microhardness loss was lowest closer to the restoration. Ketac-fil presented the highest cariostatic effect. Vitremer presented a moderate effect, while Dyract and Charisma did not differ from the control, Z250. The effects of neutral and acidulated fluoride gels were similar to each other and higher than the control. Conclusion: Conventional and resin-modified glass ionomer cements as well as neutral and acidulated fluoride gels inhibit the progression of artificial caries adjacent to restorations. The associated effect of fluoride-containing restorative materials and gels could not be demonstrated.

**Key words:** Fluorides. Dental restoration. Dental caries.

# **INTRODUCTION**

Increased life expectancies, improvements in lifestyle and the intensification of preventive interventions have all contributed towards a longer retention of natural teeth in old age. Exposed root surfaces are common in adults and older populations, generally due to gingival recession, which is associated with anatomical factors,

microbially induced periodontal diseases, surgical periodontal therapies, orthodontic movement of the teeth and various forms of trauma<sup>14,16</sup>. Exposed dentin on root surfaces becomes more susceptible to caries than enamel because of its low mineral content and its higher critical pH for dissolution<sup>8,14</sup>.

Preventive management of primary root caries lesions has a better long-term prognosis than restorative treatment. Monitoring noncavitated

lesions and reinforcing prophylactic programs must be always the choice for stopping caries progression<sup>8,14</sup>. However, when the dental anatomy and function are involved, is necessary to institute restorative treatments using materials with adequate strength, esthetics, adhesive and cariostatic effects<sup>8</sup>.

Secondary caries has been shown in studies worldwide to be the most common reason for the replacement of all types of restorations, regardless of the material used<sup>18,19</sup>. Secondary caries occur mainly at the cervical margin of restoration, where optimum hygiene conditions are difficult, and restorative techniques are sensitive and complicated by the lack of an excellent adhesion to dentin<sup>19</sup>.

Conventional glass ionomer cements (GICs), resin-modified GICs (RMGICs) and fluoride-releasing composite resins could be indicated for the restoration of root caries cavities<sup>8,30</sup>. Previous studies have suggested that the release of fluoride from a fluoride-containing material may prevent the formation of wall lesions and prevent caries at the margins of restorations<sup>10,12,24,28</sup>. The mechanisms involved in the anticariogenic effects of fluoride include the reduction of demineralization, the enhancement of remineralization<sup>5,6,15</sup>, the interference of pellicle and plaque formation and the inhibition of microbial growth and metabolism<sup>21,30</sup>.

*In vitro* studies have demonstrated the synergic effect of restorative materials in association with topical fluoride rinses or dentifrice to prevent caries adjacent to the restorations  $^{11,24}$ . Professional topical fluoride has been widely used to control the activity of caries lesions. A fluoride therapy based on daily use of fluoride gels during teethbrushing has been suggested, especially for the treatment of caries-active patients. This could add the benefit of a product with anticariogenic abilities, to the low cost and short operational time of self-applied procedures<sup>6,15</sup>. Therefore, we hypothesized that there may be an additional effect of fluoride at high concentrations on the loss of dentin microhardness around fluoride-containing restorative materials. This in vitro study compared the cariostatic effects of 5 restorative materials a conventional GIC, a RMGIC, a polyacid-modified composite resin, a resin composite with fluoride, and a resin composite without fluoride - associated with the use of neutral or acidulate fluoride gels on artificial secondary caries on root dentin. This study investigated whether there was any difference in dentin microhardness loss around fluoridecontaining restorative materials, associated with topical fluoride treatments, at different distances from the restoration margins.

## MATERIAL AND METHODS

# **Experimental Design**

A randomized complete block design was used

to evaluate the cariostatic effects of fluoridecontaining restorative materials associated with use of fluoride gels on root dentin. Blocking was a strategy used to control the variability of the dentin substrate. By using this design, the specimens formed a more homogeneous experimental unit on which to compare the treatments<sup>20</sup>. "Randomized complete" indicates that each block contains all of the treatments, applied according the randomly determined order.

The factors studied were: restorative material at 5 levels (Figure 1), topical treatments at 3 levels (Figure 1) and distance from the restoration margins at 3 levels (100, 200 and 300 mm). The experimental units were 240 bovine root specimens randomly assigned to 15 groups of treatments (n=16). Each block contained each one of all possible combinations of 5 (restorative system) x 3 (fluoride regime) groups of treatments (Figure 2). The control group of restorative system was a composite resin without fluoride (Z250, 3M ESPE Dental Products, Sumaré, SP, Brazil). Control group of topical treatments was distilled/deionized water. Acidulated fluoride gel, neutral fluoride gel and water were applied to the restoration and adjacent dentin to test the associated effect of restorative materials and gels.

The restorative materials and topical treatments were applied according to the order randomly determined by Microsoft Excel® software. The dependent variable was the Knoop microhardness (KHN) loss of root dentine around the restorations.

# **Preparation of specimens**

Two hundred and forty incisors were extracted from bovine jaws immediately after butchering. The teeth were thoroughly scaled, polished with pumice/water slurry, and washed with distilled water to clean them from debris, and were kept in a 1% chloramine-T solution for 1 week.

The roots were separated from crows and axially hemi-sectioned in a mesiodistal direction. Sections (5.0 mm x 5.0 mm x 2.0 mm) were obtained from the buccal or the lingual root surfaces at 3.0 mm from the cementonamel junction using a double-faced diamond disc (KG Sorensen Ind. e Com. Ltda, Barueri, SP, Brazil) in a low-speed handpiece under water spray coolant. Each section was embedded in epoxy resin and ground flat with a water-cooled mechanical grinder (Polipan-U, Panambra, São Paulo, SP, Brazil) with #400- and #600-grit  $Al_2O_3$  abrasive papers (Norton Abrasivos, Guarulhos, SP, Brazil).

# Cavity preparation and restorative procedures

A standard cylindrical-shaped cavity (1.5 mm depth and 2.0 mm in diameter) was prepared at the center of the flattened dentin surface using a #2294 diamond bur (KG Sorensen Ind. e Com. Ltda, Barueri, SP, Brazil) in a high-speed

Restorative system / Topical treatment	Manufacturer	Batch number
Ketac-Fil Glass-ionomer cement	3M ESPE Dental Products (Sumaré, SP, Brazil)	Powder: 142152 Liquid: 135132
Vitremer Resin modified glass-ionomer	3M ESPE Dental Products (Sumaré, SP, Brazil)	Powder: 20011019 Liquid: 20011025 Primer: 20010928 Glaze: 20011031
Dyract-Prime & Bond NT Polyacid modified composite resin	Dentsply Caulk (Milford, DE, USA)	Dyract: 0108000442 Prime & Bond NT: 3708
Charisma-GLUMA One Bond Fluoride composite resin	Heraeus Kulzer - GmbH (Gonsennheumer, Mainz, Germany)	Charisma: 060044 GLUMA One Bond: 195001
Filtek Z250-Single Bond Non-Fluoride composite resin (control)	3M ESPE Dental Products (Sumaré, SP, Brazil)	Z250 2XM Single Bond 1105
1.23% Acidulated Phosphate Fluoride gel	Vigodent (Rio de Janeiro, RJ, Brazil)	-
2% Neutral Sodium Fluoride gel	Vigodent (Rio de Janeiro, RJ, Brazil)	-
Deionized/distilled water (control)	-	-

Figure 1- The restorative materials and topical treatments applied to the specimens

Groups	Restorative Materials and Topical Treatments		
1	Ketac-Fil + 1.23% Acidulated Phosphate Fluoride gel		
2	Ketac-Fil + 2% Neutral Sodium Fluoride gel		
3	Ketac-Fil + Deionized/distilled water		
4	Vitremer + 1.23% Acidulated Phosphate Fluoride gel		
5	Vitremer + 2% Neutral Sodium Fluoride gel		
6	Vitremer + Deionized/distilled water		
7	Dyract + 1.23% Acidulated Phosphate Fluoride gel		
8	Dyract + 2% Neutral Sodium Fluoride gel		
9	Dyract + Deionized/distilled water		
10	Charisma + 1.23% Acidulated Phosphate Fluoride gel		
11	Charisma + 2% Neutral Sodium Fluoride gel		
12	Charisma + Deionized/distilled water		
13	Filtek Z250 + 1.23% Acidulated Phosphate Fluoride gel		
14	Filtek Z250 + 2% Neutral Sodium Fluoride gel		
15	Filtek Z250 + Deionized/distilled water		

Figure 2- Groups of restorative materials and topical treatments assigned within each block

handpiece under a constant water-spray coolant. The prepared cavities were treated in the following manner, according to each restorative material:

Ketac-Fil (3M ESPE): 10% polyacrylic acid was spread over the cavity for 10 s, rinsed for 30 s, and gently air-dried for 5 s, avoiding desiccation. Ketac-Fil powder and Ketac-Fil liquid were dispensed at 3.2:1 by weight, hand-mixed within 60 s, loaded into a syringe (Centrix, DFL Ind. e Com. SA, Rio de Janeiro, RJ, Brazil), and injected into the preparation. Then, the surface was covered with a polyester strip and a glass slab and pressed with a weight of 1,000 g for 30 s to extrude any excess. Seven minutes after the beginning of the mixture, the strip was removed and a surface protector (Ketac Glaze, 3M ESPE) was immediately applied and light-cured for 20 s.

Vitremer (3M ESPE): Vitremer primer was applied to the cavity preparation for 30 s, air-dried for 15 s and light-cured for 20 s. Vitremer powder and Vitremer liquid were dispensed at 2.5:1 by weight, hand-mixed within 45 s, loaded into a Centrix syringe, and injected into the preparation. Then, the surface was covered with a polyester strip and a glass slab and pressed with a weight of 1,000 g for 30 s to extrude any excess. The restoration was light cured for 40 s, the strip was removed and Vitremer finishing gloss was applied and light-cured for 20 s.

Dyract/Prime & Bond NT (Dentsply Caulk, Milford, DE, USA): 35% phosphoric acid was applied to the cavity for 15 s and rinsed for 30 s. Excess water was blotted using absorbent paper. One coat of Prime & Bond NT was applied to the cavity, left undisturbed for 30 s, blown with air for 5 s, and light-cured for 10 s. Dyract was injected into the cavity preparation, covered with a polyester strip and a glass slab, pressed with a weight of 1,000 gfor 30 s to extrude any excess and light cured for 40 s.

Charisma/GLUMA One Bond (Heraeus Kulzer, Gonsennheumer, Mainz, Germany): phosphoric acid was applied to the cavity for 20 s and rinsed for 40 s. Excess water was blotted using absorbent paper. Two consecutive coats of adhesive were applied, gently air-dried for 5 s and light-cured for 20 s. The bonded cavity was bulkfilled with Charisma, covered with a polyester strip and a glass slab and pressed with a weight of 1,000 g for 30 s to extrude any excess. After removal of the slab, the restoration was light-cured for 20 s.

Z250/Single Bond (3M ESPE): 35% phosphoric acid was applied to the cavity for 15 s and rinsed for 10 s. Excess water was blotted using absorbent paper. Immediately after blotting, 2 consecutive coats of adhesive were applied for 15 s with gentle agitation using a fully saturated applicator. After removal of the solvent by brief air-drying for 5 s, the adhesive was light-cured for 10 s. The bonded cavity was bulk-filled with Z250, covered with a polyester strip and a glass slab and pressed with a

weight of 1,000 g for 30 s to extrude any excess. After removal of the slab, the restoration was light-

The materials were light-cured using a halogen light-curing unit (XL300, 3M Dental Products, St. Paul, MN, USA) with an irradiance of 500 mW/cm<sup>2</sup>.

The specimens were stored in 100% relative humidity for 24 h at 37±1°C. Then, excess restorative material was removed using a watercooled mechanical grinder (Polipan-U) with #1000grit Al<sub>2</sub>O<sub>3</sub> abrasive paper (Norton Abrasivos). The restored fragments were cleaned with deionized/ distilled water in an ultrasonic bath for 6 min in order to remove remnants of polishing debris.

### pH-Cycling model

In order to standardize the dentin area exposed to the pH-cycling, the specimens were entirely covered with dental wax (Herpo Produtos Dentários Ltda, Rio de Janeiro, RJ, Brazil), leaving exposed only the restorations and 2.0 mm around their margins.

Each specimen was individually subjected to a demineralization/remineralization dynamic model, similar to that proposed by Featherstone, et al.9 (1986) and modified by Serra and Cury<sup>26</sup> (1992), simulating in vivo high caries activity conditions. Initially, each specimen was immersed in 5 mL remineralizing solution (Ca<sup>+2</sup> 1.5 mmol/L, PO<sub>4</sub><sup>-3</sup> 0.9 mmol/L, KCl 150 mmol/L, Tris[hydroxyme2sthyl] aminomethane 2.0 mmol/L at pH 7.0) for 24 h. After, the specimens were washed in deionized/ distilled water and immersed individually, in 5 mL demineralizing solution (Ca<sup>+2</sup> 2.0 mmol/L, PO<sub>4</sub><sup>-3</sup> 2.0 mmol/L in a buffer solution of 0.075 mmol/L of CH<sub>2</sub>COO<sup>-</sup> at pH 4.3) for 1 h. After rinsing with deionized/distilled water, 1.23% phosphate fluoride (0.03 mL), 2.0% neutral sodium fluoride (0.03 mL) or deionized/distilled water (0.03 ml) was applied to the restoration and 2.0 mm around its margins for 4 min. Then, the specimens were immersed in 5 mL of remineralizing solution, completing the 24-h cycle. Each pH-cycle totaled 24 h (demineralization: 1 h; topical treatment: 4 min; remineralization: about 23 h). Three pHcycling runs were completed during 3 consecutive days. The demineralizing and remineralizing solutions were renewed daily<sup>11</sup>.

# **Surface Knoop microhardness** measurements

Dentin surface microhardness measurements were obtained using a microhardness tester (Durimet, Ernst Leitz GmbH, Wetzlar, Germany) with a Knoop diamond and a 5 g-static-load applied for 30 s1. The surface microhardness values were measured before and after the demineralization/ remineralization cycles. Nine initial indentations (KHN<sub>1</sub>) were made at three positions: 0°, 60° and 120°; and 9 final indentations (KHN<sub>6</sub>) were made at positions 180°, 240° and 300° on dentin around the

restoration. In each position, parallel indentations were made 100, 200 and 300 mm from the margin of the restoration<sup>11</sup>. The KHN values were calculated using the following equation:

 $KHN = (14229.P) / L^2$ 

where P is the applied load (g) and L is the indentation length (mm).

# Statistical analysis

For each specimen, the mean of the nine initial indentations (KHN $_{\rm i}$ ) and the mean of the nine final indentations (KHN $_{\rm f}$ ) were considered for statistical analysis. The difference between the initial and final microhardness values (KHN $_{\rm i}$  - KHN $_{\rm f}$ ) was used to represent superficial microhardness loss on root dentin. The statistical analysis considered the mean difference between the initial and final microhardness values for each association of material and treatment at 100, 200 and 300 mm distances.

The effect of distance on root dentin microhardness loss was evaluated by Friedman's and Wilcoxon's tests ( $\alpha$ =0.05). An analysis of variance (ANOVA) tested the effects of blocking, the restorative systems, the topical treatments and their interactions for each level of the factor distance. A multiple-comparison Tukey's test ( $\alpha$ =0.05) identified possible differences in the means of microhardness values. The software SPSS 8.0 (SPSS Inc., Chicago, IL, USA) was used for the analysis.

#### **RESULTS**

A Friedman's test showed statistically significant differences among the three levels of the factor distance (p=0.007). There was a significant difference between the loss of dentin microhardness at 100 and 300 mm. (Table 1).

ANOVA revealed a significant effect of the factors blocking (p=0.000), the restorative system (p=0.000) and topical treatment (p=0.000) on the surface microhardness loss at 100, 200 and 300 mm. The interaction of particular interest (restorative system x topical treatment) was not significant at the distances of 100 (p=0.102), 200 (p=0.849) and 300 mm (p=0.580). As this interaction was not significant, factors were analyzed separately.

There were significant differences among the restorative systems at 100 (p=0.000), 200 (p=0.000) and 300 (p=0.000) mm (Table 2). At a distance of 100 mm, microhardness loss around Ketac-Fil was significantly lower than for the other restorative systems (Vitremer, Charisma, Dyract and Z250). The highest microhardness loss was observed in the non-fluoridated control material (Z250), which was similar to Charisma and Dyract. Vitremer showed a cariostatic effect lower than that of Ketac-fil, but higher than that of Dyract and Z250. At the distance of 200 mm, the effect of the restorative system was similar to that shown at 100 mm, but Vitremer did not differ significantly from

**Table 1-** Medians of the differences between initial and final dentin microhardness (KHN<sub>i</sub> - KHN<sub>f</sub>), minimum and maximum values, considering all of the restorative systems and treatments at 100, 200 and 300 mm distances

Distance from restoration margin (mm)	KHN <sub>i</sub> - KHN <sub>f</sub> (min/max)	
100	19.39° ± (-12.77/53.30)	
200	19.53ab ± (-13.09/54.93)	
300	19.56 <sup>b</sup> ± (-11.58/57.93)	

Statistical differences are expressed by different superscript letters (p< 0.05)

Table 2- Means of the differences between initial and final dentin microhardness (KHN, - KHN,) for the restorative systems evaluated at distances of 100, 200 and 300 mm

Restorative System	Means of KHN <sub>i</sub> - KHN <sub>f</sub> ± (dp)		
	100 mm	200 mm	300 mm
Ketac-Fil	12.91° ± (9.33)	13.74° ± (9.56)	15.26° ± (9.73)
Vitremer	18.77b± (10.53)	19.48 <sup>b</sup> ± (11.39)	19.48 <sup>ab</sup> ± (10.93)
Charisma	22.36 <sup>bc</sup> ± (12.14)	23.09 <sup>bc</sup> ± (13.11)	23.98bc ± (11.83)
Dyract	23.63° ± (12.52)	23.59 <sup>bc</sup> ± (12.36)	22.84 <sup>bc</sup> ± (12.44)
Z250	23.77° ± (10.35)	24.16° ± (9.96)	24.06° ± (9.48)

Means followed by distinct letters are different when compared in columns (p<0.05) Tukey dms (100 mm) = 4.41; Tukey dms (200 mm) = 4.61; Tukey dms (300 mm) = 4.41

**Table 3-** Means of the differences between initial and final dentin microhardness (KHN<sub>i</sub> - KHN<sub>f</sub>) for the topical treatments at the distances of 100, 200 and 300 mm

<b>Topical Treatment</b>	Means of (KHN <sub>i</sub> - KHN <sub>f</sub> ) ± (dp)			
	100 mm	200 mm	300 mm	
Neutral	17.73°±(11.14)	18.53°±(11.56)	19.23°±(11.33)	
Acidulate	19.16°±(10.28)	18.81°±(10.63)	18.99°±(10.10)	
Control	23.99b±(11.51)	25.08b±(11.64)	24.86b±(11.20)	

Means followed by distinct letters are different when compared in columns (p<0.05) Tukey dms (100 mm) = 2.94; Tukey dms (200 mm) = 3.06; Tukey dms (300 mm) = 2.94

Charisma and Dyract. At the distance of 300 mm, Ketac-Fil showed a significantly higher cariostatic effect than for all other tested materials except for Vitremer, from which it did not differ. Vitremer showed a cariostatic effect higher than Z250, but similar to Charisma and Dyract.

Neutral and acidulate fluoride gels did not differ significantly and showed higher cariostatic effects than the control group for all the restorative systems and distances evaluated (p=0.000) (Table 3).

### **DISCUSSION**

The cariostatic effect of fluorides is well supported by the literature. Fluorides affect caries formation through a variety of mechanisms involving the reduction of demineralization, the enhancement of remineralization, the interference of pellicle and plaque formation and the inhibition of microbial growth and metabolism<sup>5,6,15,21</sup>. Fluoride release from restorative materials is related to their matrices, setting mechanisms and fluoride content and depends on the environmental conditions<sup>3,4,7,29,30</sup>.

After topical fluoride application (>100 ppm F), loosely bound fluoride or a calcium fluoride-like material is formed. Depending on the pH of the plaque fluid, this  ${\sf CaF}_2$  layer, which has a higher solubility than hydroxyapatite and fluorapatite, will be dissolved, releasing fluoride to react with calcium and phosphate ions. The products of these reactions may be fluorapatite crystals or  ${\sf CaF}_2$  incorporated on tooth surface. This reservoir of fluoride ions is available to inhibit demineralization and enhance remineralization<sup>5,15</sup>.

In this study, the differences on cariostatic effect could be attributed to the amount of fluoride released from the restorative materials, as evaluated by dentin microhardness loss at various distances from restoration margins. Although it was not able to completely inhibit microhardness loss adjacent to the restoration, Ketac-Fil exhibited the lowest loss due to its higher fluoride-releasing properties. GIC success in reducing the production of caries-like lesions in the adjacent root surface corroborates the results obtained by other *in* 

vitro studies10,11,12,24,28. Typical GICs are materials comprised of a calcium fluoro-alumino-silicate glass powder and an aqueous solution of a poly(acrylic acid-itaconic acid) copolymer containing tartaric acid<sup>22</sup>. It is well known that the setting of these cements involves neutralization of the polyacid by the basic glass and results in the formation of an ionically cross-linked polyacrylate matrix. Initially, all of the fluoride is in the glass, but during the course of cement formation, fluoride ions are released into the aqueous acid phase and become trapped in the hardening gel matrix. Once the cement has set, the fluoride released may originate from the remaining fluoride glass, the silica gel phase, the polysalt matrix or the pore liquid in which fluoride is loosely bound and free to move7. Moreover, the erosion of GIC in an acidic environment increases the release of fluoride, which induces the formation of an acid-resistant, radiopaque, hypermineralized layer around the restorations<sup>27</sup>.

RMGICs consist substantially of GIC components (water-soluble polymeric acid, ion-leachable glass and water) together with methacrylate monomers and their associated initiation systems. These hybrid materials set partially by means of an acid-base reaction and partially by means of a polymerization reaction that is initiated by photochemical and/or chemical generation of free radicals. The action of 2-hydroxyethyl methacrylate (HEMA) as a cosolvent for organic and aqueous components affects the GIC setting reaction because ions are reluctant to form in the organic medium. Additionally, organic molecules are known to influence the conformation of the polyacrylic acid molecule<sup>22</sup>. RMGICs have the potential to release fluoride in equivalent amounts to conventional cements, but this capacity may be affected not only by the formation of complex fluoride compounds and their interaction with polyacrylic acid, but also by the type and amount of resin used for the photochemical polymerization reaction30.

In this study, under high cariogenic challenge, the ability of Vitremer to inhibit artificial caries development was observed, as dentin microhardness loss was statistically lower in this group than in the control along all distances. However, Vitremer did not inhibit caries development as effectively as Ketac-

Fil at 100 and 200 mm. The extent of the cariostatic effect provided by Ketac-Fil dropped at 300 mm and became equivalent to Vitremer. Moreover, at 200 mm and 300 mm, Vitremer behaved in the same way as Charisma and Dyract, in which fluoride release is expected to be low compared to RMGICs. Hara, et al.<sup>13</sup> (2002) demonstrated that the extent of cariostatic effects provided by conventional GICs and RMGICs was estimated to be about 300 and 150 mm, respectively, in root dentin.

The polyacid-modified composite resin (Dyract) and the composite resin with fluoride (Charisma) were shown to be ineffective in the inhibition of artificial caries lesions, as both did not differ from the control group (Z250) at all the distances. These results are in agreement with other in vitro studies<sup>11,13,28</sup>. Even though polyacid-modified composite resins have no initial fluoride "burst" effect and release lower amounts of fluoride than RMGICs, some cariostatic effect was expected for Dyract. This material does not contain water in its formulation. With time, water must diffuse from the environment toward the material before the process of glass dissolution and fluoride release can begin<sup>17</sup>. The low concentration of fluoride released by the ion-exchange mechanism and the short-term de/remineralization regimen used in this study could explain why these materials were not able to inhibit caries lesion progression around the restorations.

Obviously, in Charisma, a TEGDMA-Bis-GMA composite containing a Ba-Al-F-silicate glass filler, there is no acid-base reaction. The only source of fluoride comes from the glass filler particles, resulting in a slow diffusive release. Moreover, the polymer composition of Charisma does not contain HEMA, which would increase the hydrophilicity of the matrix and facilitate the transport of water and fluoride ions4. Composites have fluoride levels much lower than the levels released from conventional GICs or RMGICs and also somewhat lower than polyacid-modified composite resins<sup>3,30</sup>.

Under the *in vitro* simulation of high cariogenic challenge used in this study, the fluoride-containing restorative materials did not completely inhibit dentin microhardness loss around the restorations. As fluoride release from different materials may drop to very low levels after a higher initial release of ions<sup>3,4,30</sup>, fluoridation of restoratives with fluoride gels could be an interesting strategy to maintain increased levels of fluoride in surfaces with a high risk of developing caries. Some guidelines for the use of topical fluoride in high-risk patients are available. In the present study, an intensive therapeutic program was simulated with daily application of fluoride gel for 4 min<sup>6,15,25</sup>. This could be applied at home using a toothbrush or a custommade tray, or it could be professionally supervised for noncompliant home users.

The interaction of particular interest (restorative system x topical treatment) was not significant at any of the distances studied. Hence, the analysis of the effect of fluoride regimes is valid for all the materials tested. Neutral 2% NaF and 1.23% APF gels promoted a similar protection against the progression of artificial caries lesions on root surfaces. This effect is explained by the capacity of fluoride to precipitate a calcium fluoride-like layer onto tooth surfaces, which serves as a reservoir for fluoride when the pH drops<sup>30</sup>.

However, in vitro studies have also shown that 1.23% APF gel is more reactive than 2% NaF gel. CaF, formation increases in acidulate media with a consequent increase in the superficial microhardness and acid-resistance of dental structures<sup>23</sup>. Additionally, the ppmF concentration of APF gel [12,300 ppm] is higher than that of 2% NaF gel [9,040 ppm], with a higher formation of calcium fluoride-like compounds in the former. The similar cariostatic effects of neutral and acidulated fluoride gels were not expected. It is possible that the acidic pH of APF gel promoted an initial microhardness loss in root dentin in spite of the higher calcium fluoride-like compound formation.

The ability to carry out experiments under highly controlled conditions represents the major advantage of in vitro experimentation<sup>27</sup>. However, the pH-cycling model used to induce the artificial caries lesions does not take into account the effects of loss of the dentin organic phase during root caries, the effects of vital dentin reactions in vivo or the activity of salivary enzymes, thus limiting its clinical relevance. Nevertheless, the ability to quantify changes in mineral content in response to fluoride-containing materials provided information of value in assessing their potential to inhibit root caries<sup>2,23,28</sup>.

In vitro models for caries induction on root dentin can cause superficial erosions that complicate microhardness analysis. Hara, et al.11 (2002) suggested reducing the number of de/ remineralization cycles and the time of immersion in the demineralizing solution in order to avoid superficial dentin erosion. In the present study, the model proposed by Featherstone, et al. (1986) and modified by Serra and Cury<sup>26</sup> (1992) was adjusted to make it suitable for the microhardness test. Hence, the specimens were immersed in remineralizing solution for 24 h prior to submission to three cycles of de/remineralization.

The Knoop microhardness value evaluates mineral gain and loss over the course of the de/ remineralization process, taking into account the organic properties of the root dentin. This is an advantage over other methods like microradiography that quantify the mineral content of dentin and exclude the influence of the collagen matrix<sup>11-13</sup>. However, dentin is more porous and less mineralized than enamel, especially after multiple demineralizing cycles, confounding microhardness measurements. The lack of indentation uniformity can also compromise the precision of microhardness

measures. Hence, to minimize the effects of the dentin substrate on surface microhardness, a Knoop diamond with a 5 g static load was applied for 30 s<sup>1</sup> to imprint 9 initial and 9 final indentations on a representative circular area of dentin around the restoration.

### **CONCLUSIONS**

Under the conditions of this in vitro study, it was possible to conclude that fluoride-containing restorative materials as well as fluoride gel application inhibit the progression of caries-like lesions adjacent to restorations, but are not able to prevent the formation of the lesion. Conventional GICs and RMGICs reduced the microhardness loss related to artificial caries and could be recommended for root caries control, primarily in high-risk patients. The use of neutral or acidulate fluoride gels may benefit these patients, although the effects associated with restorative materials have not been demonstrated.

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